Advanced Quality Assurance instrumentation for radiotherapy: the experience at Centre for Medical Radiation Physics

Marco Petasecca, PhD



Japan 2015, 28 September, 2015 KEK



## CENTRE FOR MEDICAL RADIATION PHYSICS



## Technology SOLUTIONS

## Excellence in EDUCATION



## Partnerships in **BUSINESS**



## **Research Areas**

- Radiotherapy and Instrumentation
- External Beam Radiotherapy
- Brachytherapy
- Proton Therapy
- Heavy Ion Therapy
- Microbeam Radiotherapy
- Medical Imaging
- PET
- CT
- ProtonCT
- Volumetric dosimetry reconstruction
- Radiobiology and Dosimetry
- Personnel monitoring
- Micro and Nano dosimetry
- High Energy Physics
- Radiation detector optimisation and rad damage



## Outline

- Semiconductor Dosimetry in Proton Therapy

   LomaLinda Cancer Centre (US)
   Dose Magnifying Glass (DMG)
- 1D Si High Spatial Resolution Beam Energy reconstruction
  HIMAC (Japan)
  Serial DMG
- Dosimetry in SRT with motion compensation
  Royal North Shore Hospital (Sydney AUSTRALIA)
  MagicPlate 512
  Serial DMG
- Conclusion



## Introduction

- Advanced radiotherapy techniques such as SRT (SBRT, SRS), Proton and Heavy Ion therapy produce:
  - high dose modulation and tight gradients
  - Strong hypo-fractionation with small or none margin of error
  - Conformality requires organ motion compensation → interplay effects
- Difficulties in the dosimetric verification of these new complex treatment methods using existing dosimeters has led to the need for a new generation of fast responding real time dosimeters with sub-millimetre accuracy
- Most of them are spin off from HEP radiation detectors designed for fundamental research.



## Dose Magnifying Glass (DMG)

- The DMG is a silicon strip detector
  - Designed and developed at CMRP
- Real time and high spatial resolution
- Each diode provides sensitive area 20 x 2000 μm<sup>2</sup> and 200 μm pitch, mounted on 375μm thick p-type Substrate

# 



#### Authors:

- CMRP: J. Wong, I. Fuduli, M. Newall, M. Petasecca, M. Lerch, S. Guatelli, A. Rosenfeld,
- Loma Linda university: A. Wroe and R. Schulte

## The Data Acquisition System (DAS)

 Very large scale integration application specific integration circuit (VLSI ASIC) known as; TERA.



 Connected to a field programmable gate array (FPGA) with universal serial bus (USB) interface to a personal computer (PC).



 The detector is operated in passive mode.

 The TERA DAS consists of a <u>current to frequency converter and</u> <u>digital counter</u> enabling *continuous integration and readout of the response from 256 channels* during acquisition [5].

## Setup at LMCC

- The DMG is positioned horizontally in front of the nozzle
- Measures simultaneously profile and depth dose in a water phantom
- Waterproof
- Automatic stager for depth scanning
- 127or 157 MeV protons
- 20 mm diameter proton beam, comparison with a commercial PTW diode, PTW Markus Parallel-Plate Ionization Chamber and Monte Carlo



## Results – PDD 127 MeV



0.0L

20

40

60

Position (mm)

80

100

Submitted to PMB – Aug 2015

## Results – PDD 157 MeV







## Results – Profiles 127 and 157 MeV



0.0

4 6 8 10 Position (mm)

0.0

10

Position (mm)

### Beam Energy reconstruction in C-12 RT at HIMAC

#### introducing Serial DMG



Figure – Serial Dose Magnifying Glass (sDMG) [3].

#### **Experimental Methodology**

- Experiments conducted at HIMAC, Chiba, Japan. The detector is irradiated by;
  - C-12 ion beam,
  - Energy 290 MeV/u (E') and
  - 10x10cm<sup>2</sup> square field
- Placed inside a PMMA phantom, the detector is setup in configurations:
- 1. Detection axis aligned **parallel** to beam direction
- 2. Detection axis aligned **perpendicular** to beam direction



#### Experimental Methodology – Depth Profile

- The detection axis is aligned **parallel** to the direction of the C-12 beam.
- C-12 ion beam, energy 290 MeV/u and 10x10cm<sup>2</sup> square field.
  - PBP (pristine Bragg peak)
  - SOBP (spread-out Bragg peak, 60mm width in water)
- **Depth Dose Profiles: PBP** measurements conducted with increasing depth in PMMA (+/- 1mm).







sDMG detector in PMMA

C-12 beam



### Experimental Methodology – Lateral Profile

Common Axis The detection axis is aligned **perpendicular** to the direction of the of Detection C-12 beam. Various depths SOPB (60mm width in water) C-12 ion beam, energy 290 MeV/u of PMMA and **10x10cm<sup>2</sup>** square field. Beam,  $E_0$ Penumbral Study: Measurements conducted with increasing depth in PMMA (+/-1mm). Data Acquisition System D sDMG detector in C-12 beam **PMMA** 

#### Results: Pristine Bragg Peak - Measurement

• Result processed with generated equalisation vector.



Acquisition of PBP for various PMMA depths, with equalisation

- Larger straggling effect in silicon?
- Radiation damage creates artefacts?

#### **Results: Energy Reconstruction**

- Propose method of independent beam energy verification.
- Calculation of E<sub>0</sub> (residual energy of beam, at surface of PMMA phantom) from PBP measurements.



#### Results: Energy Reconstruction - MC



0.1mm

#### **Results: Energy Reconstruction**

- Measurement of location of PBP in silicon detector (at known depth in PMMA). 1.
- Energy (E<sub>1</sub>) upon entrance to silicon is back-2. calculated from measurement of PBP.
- 3. Location of **PBP** (projected range without silicon + depth) in PMMA is determined from **E**<sub>1</sub>.
- 4. Residual Energy  $(E_0)$  at entrance to PMMA phantom calculated from location of PBP in PMMA (without silicon)



4. Energy of C-12 at PMMA Phantom Surface - SRIM

Projected Range in PMMA (mm)

Workflow Diagram



#### **Results: Energy Reconstruction**



Depth in PMMA (mm), (+/- 1 mm)	Measured Peak Location in Silicon (mm), (+/- 0.4mm)	Reconstructed Energy, <b>E</b> <sub>1</sub> (MeV/u), (+/-3MeV/u)	Simulated Energy (MeV/u), (+/-0.1%)	Reconstructed Residual Energy, <b>E</b> ₀, (MeV/u), (+/- 3MeV/u)	Percentage Difference to Monte-Carlo (%)
102	19.4	118	121	279	1.62
89	27.2	143	147	277	1.25
64	42.1	186	190	277	0.93
54	48.7	203	206	278	1.30

- E<sub>0</sub> determined by Monte-Carlo simulation to be **275 MeV/u +/- 0.01%**,
- E<sub>0</sub> determined by reconstruction to be (278 +/- 1) MeV/u

#### Results: Penumbral Study

 SOPB (60mm width in water) delivered for depths in PMMA; 60mm, 80mm, 100mm, 120mm and 130mm.

Penumbral Profiling of C-12 Ion Beam in PMMA

1.0 60mm PMMA 1.0 60mm PMMA 0.9 80mm PMMA 80mm PMMA 100mm PMMA 100mm PMMA 0.8 120mm PMMA The Western 0.8 130mm PMMA 120mm PMMA Normalised Response 0.7 Normalised Response 130mm PMMA 0.6 0.6 0.5 0.4 0.4 0.3 0.2 0.1 0.2 0.0 14 12 0 10 Depth in PMMA (cm) 0.0 Distance (cm) 0.0 0.5 1.0 1.5 2.0 2.5 2 **Distance** (cm) 0 3

#### Penumbral Profiling of C-12 Ion Beam in PMMA

#### Results: Dose-Rate dependence

n

12

16 20 24 28

- Investigated dose-rate dependence of detector under irradiation by SOBP (width 60mm in water).
- Region of SOBP detector is exposed to, high-LET particles







0

12

16 20

24 28

Time (s)

32 36

40

32 36 40

Time (s)

#### Results: Dose-Rate Dependence



#### Future Work

Pristine Bragg Peak results demonstrated:

#### Prolonged Exposure $\rightarrow$ Radiation Damage

- Necessitates implementation of <u>radiation harder substrate</u>
- Penumbral study and Pristine Bragg Peak results established feasibility of high spatial resolution silicon detector.
- But, necessitates <u>simultaneous measurement of</u> <u>depth dose profile and beam profile</u>
- Thus, future studies will utilise **DUO**:
  - a two dimensional detector for high resolution profiling, enabling simultaneous readout of X and Y profiles



# Stereotactic RT and motion tracking compensation study using MP512

Designed and developed at **CMRP**, MP512 is a 2D array:

- Monolithic silicon:
  - **512** diodes in a square array
  - Sensitive volume ~ 0.5 x 0.5 x 0.1 mm<sup>3</sup>
  - Diode separation 2 mm
  - Size 52 x 52 mm<sup>2</sup>
- Readout Electronics:
  - Custom design multi-channel electrometer
  - Pulse-by-Pulse acquisition





## Dosimetric Characterisation of MP512: OF – PDD in 6MV photon beams

• MP512 compared to various dosimeters for varying field size.

Condition	Value		
Source	Linear Accelerator		
Туре	6MV photon		
Dose delivered	100 MU		
Field Size	•••		
Source to surface distance	90 cm		
Depth	10 cm		

 For field sizes < 1x1cm<sup>2</sup> MP512 over responds <4%, for greater field sizes, results agree within +/- 1%.





Figure – Normalised output factor measurements of 6MV beam for a variety of detectors (Aldosari et. al. 2014)

## Combining Small Field dosimetry and Motion Tracking

• Characterize the performance of a *high spatial* 







## **Dynamic Characterisation of MP512**





• Introduction of **motion tracking system** and **MLC tracking** throughout beam delivery to moving system → **Motion+Tracking** 

## **Dynamic Characterisation of MP512**

#### Without Motion – 1x1cm<sup>2</sup> field size





## **Dynamic Characterisation by MP512**

#### With Motion – 1x1cm<sup>2</sup> field size

Y-Channel Number





#### With Motion and MLC Tracking - 1x1cm<sup>2</sup> field size





ntegral Response (Counts)

## sDMG – FS 1x1cm<sup>2</sup>



## **Results: Beam Profiles**

Comparison of results from **MP512** to **EBT3 film** for three experimental cases for field size 1x1cm<sup>2</sup>.



Y-profiles – 1x1cm<sup>2</sup>

Figure – Normalised profile comparison, MP512 with EBT3 film ()

The average uncertainty for EBT3 film is +/-1.9%, for M512 is +/-2%, induced by the RF ٠ from Calypso



## **Results: Beam Profiles**

Comparison of results from MP512 to EBT3 film for three experimental cases for field size 1x1cm<sup>2</sup>.
 <u>X-profiles – 1x1cm<sup>2</sup></u>



Figure – Normalised profile comparison, MP512 with EBT3 film ()



## **Results – MLC Dynamic Wedge**

 MLC used to produce enhanced dynamic wedge to generate an intensity modulated dose profile

- Integral profile along y-axis is compared for cases:
  - Without Motion
  - With Motion
  - With Motion + Tracking





## Detailed timing information



## Timing analysis of motion/interplay effect



Integral charge distribution profile (nC)

180

140 -120 -100 -80 -60 -40 -20 -

20

Distance along Y axis (mm)

30

Motion compensation
 algorithm/tracking software
 generates a lag in time (200 ms)
 → tracking cannot cope with fast
 transient components

 Integral profiles cannot display which is the phenomenon which creates the dose discrepancy



# **MMND & IPCT 2016**

Mini-Micro-Nano-Dosimetry and New Technologies for Prostate Cancer Treatment International Workshops

> 25<sup>TH</sup> – 30<sup>TH</sup> JANUARY HOBART, TASMANIA